## SLOVAK UNIVERSITY OF TECHNOLOGY IN BRATISLAVA

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WORKSHOP: DISCRETE DUALITY FINITE VOLUME METHOD AND APPLICATIONS

# The image segmentation and cell tracking in macrophage data



## Macrophages?

Sipka, Tamara, et al. "Macrophages undergo a behavioural switch during wound healing in zebrafish." *Free Radical Biology and Medicine* (2022).





## Macrophages in microscopy videos – from Montpellier University

#### Site of wound



#### Site of wound



## **Procedure of macrophage segmentation & tracking**



**1.** Filtering by considering the temporal coherence

2. Segmentation by using local thresholding and removal of the remaining noise

- 1. Extraction of trajectories when segmented cells overlap in time
- 2. Connection of trajectories obtained from #1 by approximating the direction of the cell movement.

Image segmentation of macrophages - space-time filtering Sarti, Alessandro, Karol Mikula, and Fiorella Sgallari. , IEEE Transactions on Medical Imaging (1999), "Nonlinear multiscale analysis of three-dimensional echocardiographic sequences."

$$\frac{\partial u}{\partial t} = clt(u) \nabla \cdot \left( g(|\nabla G_{\sigma} * u|) \nabla u \right)$$

$$g(s) = \frac{1}{1 + Ks^2}, K > 0, s = \nabla u$$

To measure the time coherence for moving objects

$$clt(u) = \min_{w_1,w_2} \frac{1}{(\Delta\theta)^2} \left( | < \nabla u, w_1 - w_2 > | + |u(\mathbf{x} - w_1, \theta - \Delta\theta) - u(\mathbf{x}, \theta)| + |u(\mathbf{x} + w_2, \theta + \Delta\theta) - u(\mathbf{x}, \theta)| \right)$$

 $w_1, w_2$ : arbitrary vectors in space

 $\theta$ : time increment between discrete time slices

 $clt \rightarrow 0$  at a pixel (i, j) There is motion coherence (objects)

*clt*  $\rightarrow$  large at a pixel (i, j) There is no motion coherence (noise)

Image segmentation of macrophages - space-time filtering



- Discretization of space-time filtering equation

By using the semi-implicit scheme,

$$\frac{u_k^{n+1} - u_k^n}{\tau_F} = clt(u_k^n)\nabla \cdot \left(g(|\nabla u_k^{\sigma;n}|)\nabla u_k^{n+1}\right), \qquad u_k^n(\mathbf{x}) = u(n\tau_F, \mathbf{x}, k\Delta\theta) \quad \text{: Numerical solution in } k^{th} \text{ time frame in } n^{th} \text{ filtering step}$$

By using the diamond cell approach,



$$\nabla^{1,0} u_{i,j,k}^{n} = \frac{1}{h} (u_{i+1,j,k}^{n} - u_{i,j,k}^{n}, u_{i,j,k}^{1,1} - u_{i,j,k}^{1,-1}), \qquad \nabla^{-1,0} u_{i,j,k}^{n} = \frac{1}{h} (u_{i-1,j,k}^{n} - u_{i,j,k}^{n}, u_{i,j,k}^{-1,1} - u_{i,j,k}^{-1,-1}),$$

$$\nabla^{0,-1} u_{i,j,k}^{n} = \frac{1}{h} (u_{i,j,k}^{1,-1} - u_{i,j,k}^{-1,-1}, u_{i,j-1,k}^{n} - u_{i,j,k}^{n}), \qquad \nabla^{0,1} u_{i,j,k}^{n} = \frac{1}{h} (u_{i,j,k}^{1,1} - u_{i,j,k}^{-1,1}, u_{i,j+1,k}^{n} - u_{i,j,k}^{n}),$$

$$u_{i,j,k}^{n+1} = u_{i,j,k}^{n} + \frac{\tau_{F}}{h^{2}} clt(u_{i,j,k}^{n}) \sum_{|l|+|m|=1} g(|\nabla^{l,m} u_{i,j,k}^{\sigma;n}|)(u_{i+l,j+m,k}^{n+1} - u_{i,j,k}^{n+1})$$

$$l, m \in \{-1, 0, 1\}, |l| + |m| = 1$$

- Local Otsu's method (thresholding)

Calculation of the optimal threshold using global Otsu's method in a local window

#### **Global Otsu's method**

Let us suppose there are two classes,  $C_0$  and  $C_1$  represented by a threshold intensity k.

OTSU, N.: A threshold selection method from gray-level histograms, IEEE transactions on systems, man, and cybernetics 9(1) (1979), 62-66.



Searching for a threshold  $T_r$  that maximizes  $\sigma_B^2(T_r)$ 

$$\sigma_B^2\left(T_r^*\right) = \max_{0 \le T_r < L} \sigma_B^2\left(T_r\right)$$

Variance between two classes is defined by

$$\sigma_B^2(T_r^*) = \frac{\left(\mu_T \omega(T_r) - \mu(T_r)\right)^2}{\omega(T_r)(1 - \omega(T_r))}$$

 $\omega_{\#}$ : probability of class # , #=0,1  $\mu_{\#}$ : mean of class # , #=0,1

#### Image segmentation of macrophages - Local Otsu's method

The optimal threshold in a certain window of size  $s \times s$  for every pixel centered in (i, j) is calculated



#### Image segmentation of macrophages - Global Otsu's method



- Local Otsu's method without space-time filtering



Image segmentation of macrophages - Local Otsu's method <u>with</u> space-time filtering







Original



Adjusted



Space-time filtering+Local Otsu's



- The Subjective surface segmentation (SUBSURF) method

The SUBSURF method **remove the artifact** from the local Otsu's method and **smooth the inside of macrophages** 

$$u_t = |\nabla u| \nabla \cdot \left(g \frac{\nabla u}{|\nabla u|}\right) \qquad g(s) = \frac{1}{1 + Ks^2}, \ K > 0, \quad s = |\nabla G_\sigma * I^0|$$

The final discretization form is given by

$$\begin{split} u_{ij}^{n+1} - u_{ij}^n &= \frac{\tau}{h^2} \bar{Q}_{ij}^{lm;n} \sum_{|l|+|m|=1} g_{ij}^{lm,\sigma} \frac{u_{i+l,j+m}^{n+1} - u_{ij}^{n+1}}{Q_{ij}^{lm;n}} \\ Q_{ij}^{lm;n} &= \sqrt{\epsilon^2 + |\nabla^{lm} u_{ij}^n|^2} \qquad \bar{Q}_{ij}^{lm;n} = \sqrt{\epsilon^2 + \frac{1}{4} \sum_{|l|+|m|=1} |\nabla^{lm} u_{ij}^n|^2}} \end{split}$$

- The Subjective surface segmentation (SUBSURF) method

Adjusted

Space-time filtering+Local Otsu's



Filtering+Local Otsu's+SUBSURF





- Comparison with deep learning-based segmentation



Stringer, Carsen, et al. "Cellpose: a generalist algorithm for cellular segmentation." *Nature methods* 18.1 (2021)

von Chamier, Lucas, et al. "Democratising deep learning for microscopy with ZeroCostDL4Mic." *Nature communications* 12.1 (2021)

- Comparison with deep learning-based segmentation



- The approximate center of the cell

Time-relaxed eikonal equation:  $\left| oldsymbol{\nabla} d 
ight| = 1$ 





#### - The approximate center of the cell

We solve the unknown function  $d(\mathbf{x}, t, \theta)$ ,  $(\mathbf{x}, t) \in \Omega \times [0, T_E]$ 

By using Rouy-Tourin scheme, (in 2D+time)

$$d_{ij}^{n+1}(\theta) = d_{ij}^{n}(\theta) + \tau_D - \frac{\tau_D}{h} \sqrt{M_{ij}^{10}(\theta) + M_{ij}^{01}(\theta)}$$

$$M_{ij}^{10}(\theta) = \max\left(D_{ij}^{-1,0}(\theta), D_{ij}^{1,0}(\theta)\right)$$
$$M_{ij}^{01}(\theta) = \max\left(D_{ij}^{0,-1}(\theta), D_{ij}^{0,1}(\theta)\right)$$
$$D_{ij}^{lm}(\theta) = \left(\min\left(d_{i+l,j+m}^{n}(\theta) - d_{ij}^{n}(\theta), 0\right)\right)^{2}$$
$$l, m \in \{-1, 0, 1\}, \ |l| + |m| = 1.$$

- The approximate center of the cell



- Extraction of trajectories

## **Partial trajectories**

Case 1: when the cells are *mostly* overlapped in temporal direction

Case 2: when the cells are *barely* overlapped in temporal direction

Case 3: when the cells are *not* overlapped in temporal direction

- Extraction of partial trajectories



## Approximate centers are connected when the cells are overlapped in time

Steps for extracting partial trajectories



- Extraction of partial trajectories

Case 1: when the cells are *mostly* overlapped in temporal direction



- Extraction of partial trajectories

Case 2: when the cells are *barely* overlapped in temporal direction



- Extraction of partial trajectories

The steps are repeated until every cell is inspected for forming partial trajectories

#### - Extraction of partial trajectories





- Connection of partial trajectories

## We assume that the reason for non-overlapping cells is that their *movement is relatively fast*.

→ non-overlapping cells keep their direction of movement.

- Connection of partial trajectories

The tangent is computed by third order accuracy using finite difference approximation



$$V^{b}(\mathbf{r}_{\theta}) = \frac{1}{\Delta\theta} \left( \frac{11}{6} \mathbf{r}_{\theta} - 3\mathbf{r}_{\theta-1} + \frac{3}{2} \mathbf{r}_{\theta-2} - \frac{1}{3} \mathbf{r}_{\theta-3} \right), \quad V^{f}(\mathbf{r}_{\theta}) = \frac{1}{\Delta\theta} \left( -\frac{11}{6} \mathbf{r}_{\theta} + 3\mathbf{r}_{\theta+1} - \frac{3}{2} \mathbf{r}_{\theta+2} + \frac{1}{3} \mathbf{r}_{\theta+3} \right)$$

 $\mathbf{r}_{\theta} = (x_{\theta}, y_{\theta})$  point of the partial trajectory at  $\theta$ 

- Connection of partial trajectories



Under the assumption,  $V^{f}(\mathbf{r}_{a-1}) = V^{f}(\mathbf{r}_{a})$ 

$$\mathbf{r}_{a-1} = -\frac{6}{11} V^{f}(\mathbf{r}_{a}) \cdot \Delta\theta + \frac{18}{11} \mathbf{r}_{a} - \frac{9}{11} \mathbf{r}_{a+1} + \frac{2}{11} \mathbf{r}_{a+2},$$

Under the assumption,  $V^b(\mathbf{r}_{b+1}) = V^b(\mathbf{r}_b)$ 

$$\mathbf{r}_{b+1} = \frac{6}{11} V^b(\mathbf{r}_b) \cdot \Delta\theta + \frac{18}{11} \mathbf{r}_b - \frac{9}{11} \mathbf{r}_{b-1} + \frac{2}{11} \mathbf{r}_{b-2}$$

#### - Connection of partial trajectories

If there is a trajectory near the estimated point  $\mathbf{r}_{es}$ , i.e.,  $|\mathbf{r}_{es} - \mathbf{r}_i| < \Delta \mathbf{r}$ 

The trajectory is linked to the trajectory containing point  $r_i$ 



- Connection of partial trajectories



## **Result - 1<sup>st</sup> dataset of macrophages**

 $accuracy = \frac{\# \ of \ correct \ links}{\# \ of \ total \ links}$ 

*Mean accuracy*  $\approx 0.975$ 



## **Result - 2<sup>nd</sup> dataset of macrophages**



Mean accuracy  $\approx 0.974$ 



#### Cell tracking- quantitative analysis by using the mean Hausdorff distance

1 pixel=0.326µm

## Conclusion

- Combination of space-time filtering, local Otsu's, and SUBSURF method **segmented all macrophages** having high variability of the image intensity
- The proposed cell tracking method traces the movement of cells by considering **overlap of cell bodies** in the temporal direction and **the approximate direction** of the movement.

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